



Many for one rank

Calibration-free, accelerated dynamic MRI based on rank-one matrix recovery

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Outline

- Motivation
 - Compressed sampling for accelerated MRI
 - Parallel, multichannel imaging
 - Dynamics
- Blind deconvolution
 - Methods for fully sampled data
- Dynamic MRI + blind deconvolution
 - Joint channel and image estimation as rank-one recovery
 - Experimental results

Motivation: Accelerated MRI







Dynamic MRI Sequence of images with similarities across space and time

Compressed sampling Subsample k-space to accelerate data acquisition Naïve reconstruction (Zero-filled inverse FFT) Spatial aliasing due to undersampling in k-space

Obviously, reconstruction with sparse and low-dimensional signal models that exploit spatial and temporal structures will provide better reconstruction [Lustig et al., *Sparse MRI*, MRM, 2007]

Problem description

Calibration-free: Jointly estimate MR image sequence and coil sensitivity profiles from under-sampled data











Known coil sensitivity responses Unknown dynamic MRI sequence

$$y_t^c = R_{\Omega_t} \mathcal{F} \Sigma_{s_c} \boldsymbol{x_t}$$

A system of linear equations !!!



$$y_t^c = R_{\Omega_t} \mathcal{F}(s_c \odot x_t)$$

Stack all measurements into a linear system [Pruessmann et al. SENSE, MRM, 1999]



Frame-by-frame reconstruction Oversampling in space due to redundant coils helps with the reconstruction



$$y_t^c = R_{\Omega_t} \mathcal{F}(s_c \odot x_t)$$

Stack all measurements into a linear system [Pruessmann et al. SENSE, MRM, 1999]

8X subsampled k-space

Frame-by-frame reconstruction Multiple coils/channels provide redundancy to offset small subsampling factors only



Dynamic MRI A video sequence with similarities across space and time



Small region with significant action Spatial and temporal redundancies (like videos)





Parallel MRI

$$y_t^c = R_{\Omega_t} \mathcal{F}(s_c \odot x_t)$$

$$x_{t+1} \approx F_t x_t$$

Motion-adaptive constraint

8X subsampled k-space





Motion-adaptive reconstruction

Exploit temporal structure in the reconstruction

[Jung et al., k-t FOCUSS, MRM, 2009; Asif et al., MASTeR, MRM, 2013]

Autocalibration?



Unknown coil sensitivity responses $y_t^c = R_{\Omega_t} \mathcal{F}_{\Sigma_{s_c}} x_t$ Unknown dynamic MRI sequence

A system of bilinear equations !!!

Blind deconvolution: fully sampled data

• A common technique in blind deconvolution schemes is to exploit *cross-relation consistency*:

Consider a multi-channel system

 $y_i = x \circledast h_i$ for $i = 1, 2, \ldots$

Cross-relation consistency:

$$y_i \circledast h_j = y_j \circledast h_i$$
 for all i, j

The null-space of the matrix defined by these equations provides all the feasible solutions

[Tong et al., 1991; Harikumar & Bresler, 1999; ...]

MRI autocalibration: fully sampled regions

 Conventional coil estimation methods use a small, fully sampled k-space region



• With the exception of SAKE, all these methods require a small, fully sampled region in the k-space

[Sodickson et al., *SMASH*, MRM, 1997; Griswold et al., *GRAPPA*, MRM, 2002; Lustig et al., *SPIRIT*, MRM, 2010; Uecker et al., *ESPIRIT*, MRM, 2014; Shin et al., *SAKE*, MRM, 2014]

Autocalibration?



Unknown coil sensitivity responses $y^c_t = R_{\Omega_t} \mathcal{F} \Sigma_{s_c} x_t$ Unknown dynamic MRI sequence

A system of bilinear equations !!!

Blind deconvolution + dynamic MRI

Stack all the measurements into a large system:

$$y_t^c = R_{\Omega_t} \mathcal{F}(s_c \odot x_t) \Big|_{\substack{c=1,\dots,C\\t=1,\dots,T}} \longrightarrow y = \mathcal{A}(xs^*)$$

Sample diagonal entries of the rank-1 matrix: xs^st

$$xs^* = \begin{bmatrix} x_1 \\ \vdots \\ x_T \end{bmatrix} \begin{bmatrix} s_1^* & \dots & s_C^* \end{bmatrix} = \begin{bmatrix} x_1s_1^* & \dots & x_1s_C^* \\ \vdots & \ddots & \vdots \\ x_Ts_1^* & \dots & x_Ts_C^* \end{bmatrix}$$

Blind deconvolution + dynamic MRI

Solve a nonlinear problem for rank-1 recovery

minimize
$$||x||_2^2 + ||s||_2^2$$
 s.t. $y = \mathcal{A}(xs^*)$

Low-rank factorization for matrix completion/reconstruction [Recht et al., 2010; Burer & Monteiro, 2005; Jain et al., 2013; Cai et al., 2010; ...]

Add motion-adaptive prior:

 $\underset{x,s}{\text{minimize }} \|x\|_{2}^{2} + \|s\|_{2}^{2} + \sigma \|y - \mathcal{A}(xs^{*})\|_{2}^{2}$

$$+\lambda \sum_{t=1}^{T-1} \|x_{t+1} - F_t x_t\|_2^2$$

Known sensitivity maps



Unknown sensitivity maps



With motion

R=4

Without motion





Known sensitivity maps



Unknown sensitivity maps



With motion





R=8

Without motion

Known sensitivity maps Unknown sensitivity maps

R=4

Without motion









Known sensitivity maps Unknown sensitivity maps

R=8

Without motion









Summary

Calibration-free: Jointly estimate MR image sequence and coil sensitivity profiles from under-sampled data



References

- M. Asif, L. Hamilton, M. Brummer, J. Romberg, *Motion-adaptive spatiotemporal regularization (MASTeR) for accelerated dynamic MRI*, Magnetic Resonance in Medicine, September 2013
- M. Asif, F. Fernandes, J. Romberg, *Low-complexity video compression and compressive sensing*, Asilomar 2013
- A. Ahmed, B. Recht, J. Romberg, *Blind deconvolution using convex programming*. IEEE Trans. Info. Theory, March 2014.

Data and codes: http://users.ece.gatech.edu/sasif/dynamicMRI http://dsp.rice.edu/

Backup slides

R=4

Fully-sampled (ground truth)



Without motion

R=8

Fully-sampled (ground truth)



Without motion

R=4

Fully-sampled (ground truth)

Without motion



R=8

Fully-sampled (ground truth)

Without motion

